



# Optical coherence tomography based on induced coherence with a pulsed pump

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## 1. Graphical Abstract

### OCT based on induced coherence with a pulsed pump

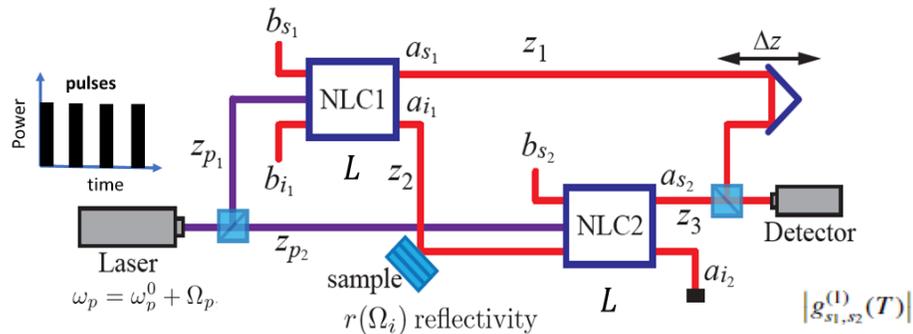
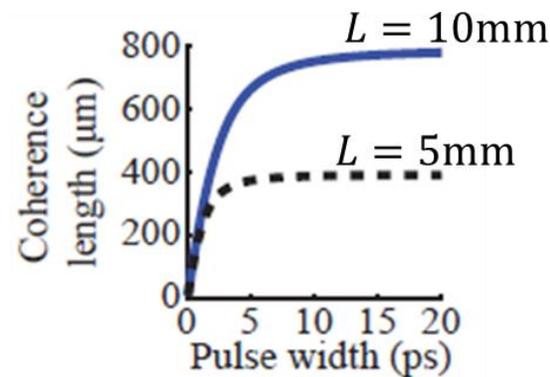
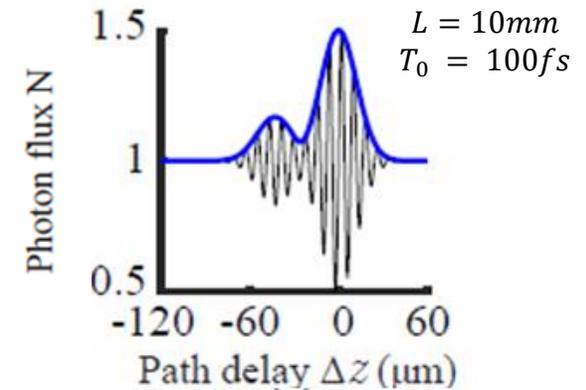


Fig. Simplified sketch of ICT. We considered MgO-doped LiNbO<sub>3</sub> crystals.  $\lambda_p = 532 \text{ nm} \rightarrow \lambda_s = 810 \text{ nm}$  and  $\lambda_i = 1550 \text{ nm}$  with  $D = -263.50 \text{ fs/mm}$  and  $D_+ = 780 \text{ fs/mm}$ .  $T_2 = 0$ .

### The first-order correlation function:



### Optical depth sectioning of a Bi-layer sample



# 2. Introduction

Optical Coherence Tomography based on induced coherence is an optical depth sectioning technique based on the interference of the signal photons from two downconverters. In this regime the down-converted photons show frequency anticorrelation.

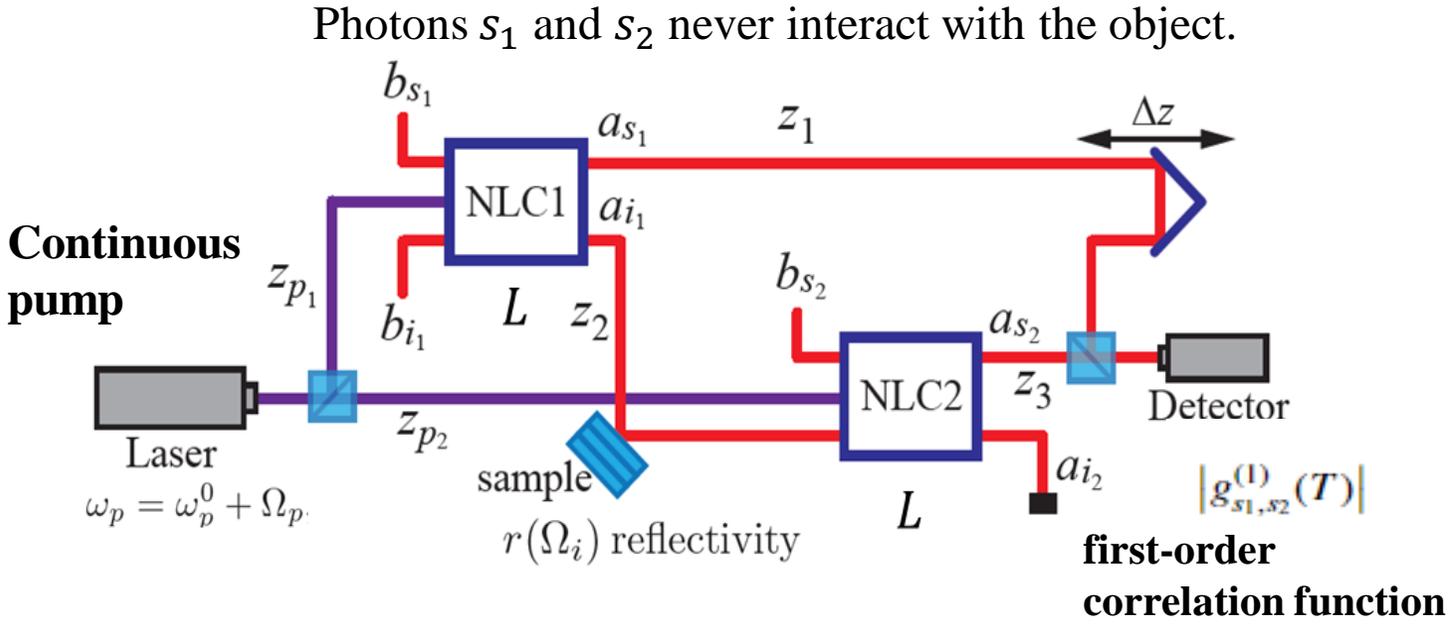


Fig. Simplified sketch of ICT. NLC stands for nonlinear crystal, s and i are labels that designate signal and idler modes, b and a represent input/output quantum operators..  $D = N_i - N_s$ :  $N_{s,i}$  inverse group velocities

**Bi-layer object**

$$|g_{s1,s2}^{(1)}(T)| = \text{tri} \left\{ \frac{1}{DL} [T - T_0] \right\}$$

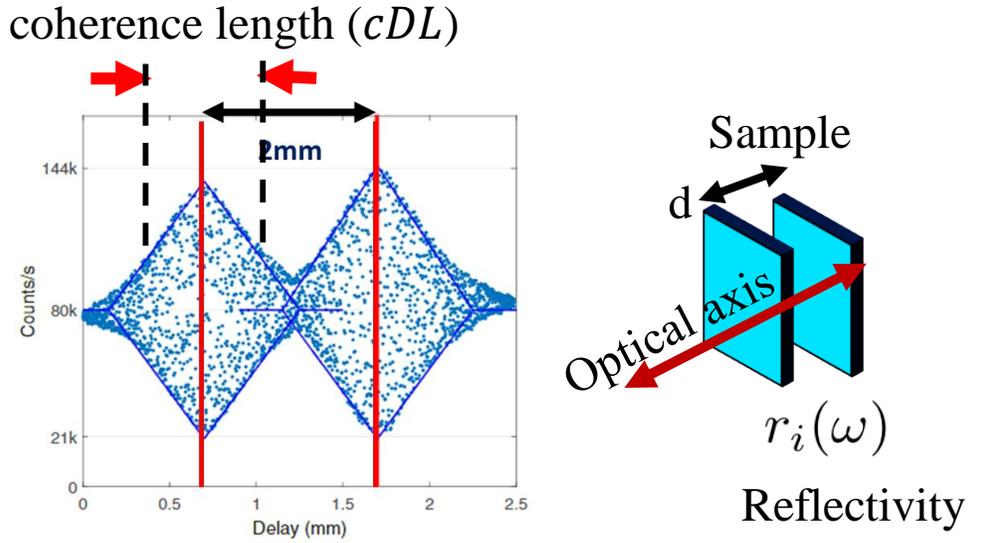


Fig. Interferogram from two layers separated 1 mm apart with a resolution of 600 $\mu$ m

### 3. Is the frequency anticorrelation provided by continuous Parametric Down Conversion a requisite to do OCT based on induced coherence?

**NO.** We show that one can do OCT with pulsed pump

#### The correlation function

is very weakly dependent on the laser pulse width ( $T_0$ )

$$|g_{s_1, s_2}^{(1)}(T)| = \text{Tri} \left( \frac{T}{DL} \right) \exp \left[ -\frac{1}{16} \left( 1 - \frac{2D_+}{D} \right)^2 \frac{T^2}{T_0^2} \right]$$

$D = N_i - N_s; N_{s,i}$  inverse group velocities of the photons

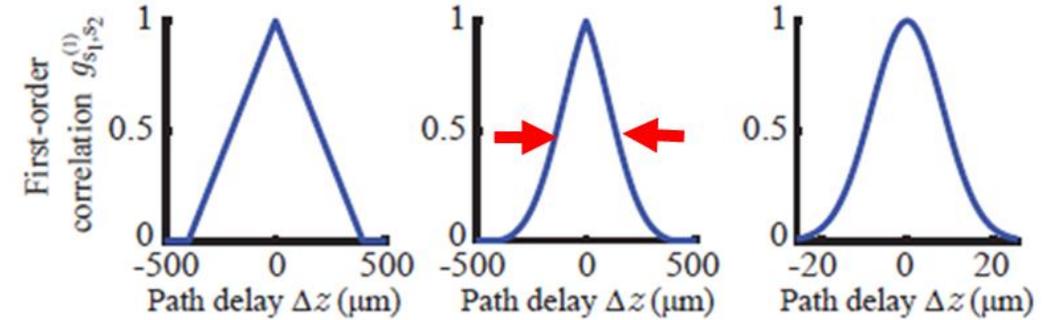
#### Frequency-entangled photons

We observe coherence for all values of the degree of entanglement between the signal and idler beams.

Biphoton function

$$\Phi(\Omega_s, \Omega_i) = \left( \frac{\alpha T_0 DL}{\sqrt{2\pi}} \right)^{1/2} \exp \left[ -\frac{(\Omega_s + \Omega_i)^2 T_0^2}{2} \right] \times \exp \left[ -\frac{\alpha^2 (DL)^2}{16} (\Omega_s - \Omega_i)^2 \right].$$

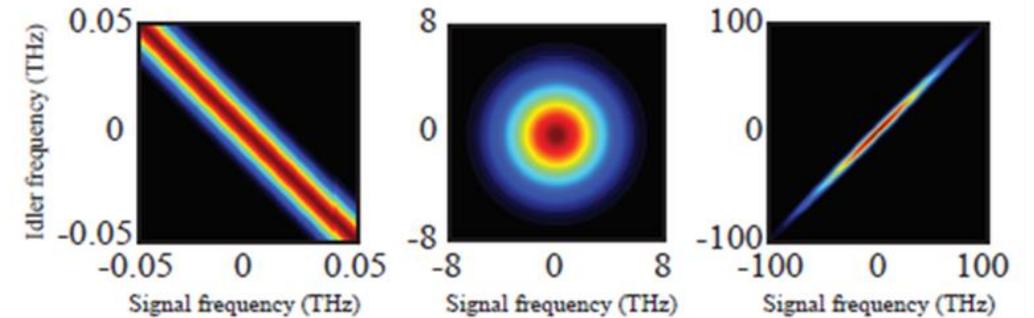
$$\text{Degree of entanglement } \gamma = \frac{cDL}{2\sqrt{2}T_0}$$



$T_0 = 100\text{ps}$

$T_0 = 2\text{ps}$

$T_0 = 100\text{fs}$



$\gamma \gg 1$

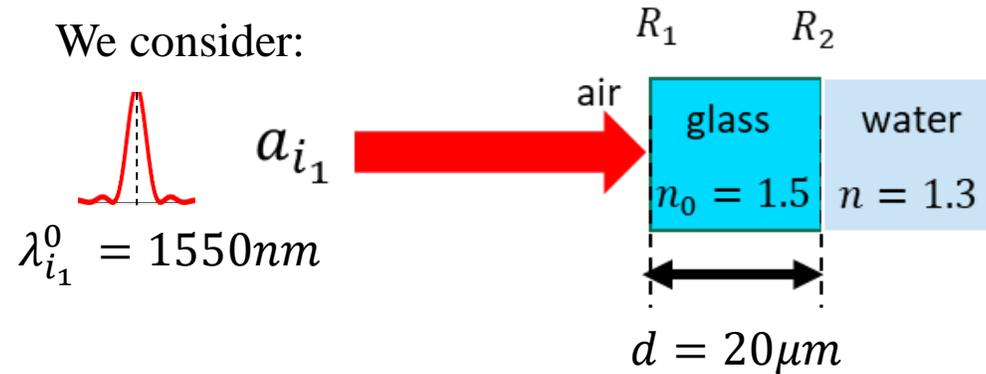
$\gamma = 1$

$\gamma \ll 1$

Fig. (Up) First order correlation function. (Down) Normalized biphoton function  $|\Phi|^2$ .

# 4. Can the use of pulsed pumps allow the use of longer crystals without reducing the bandwidth?

## Bi-layer sample resolution.



$R_1$  and  $R_2$  are the reflectance of the first and second layer of the sample.

The signal detected at one output port of the beam splitter is

$$N = N_{s_1} \left\{ 1 + r_0 g_{s_1, s_2}^{(1)}(T_1, T_2) \sin \left[ (\omega_p^0/c)(z_{p_2} - z_{p_1}) - (\omega_i^0/c)(z_2 + n_i L) - (\omega_s^0/c)(z_1 - z_3) \right] \right. \\ \left. + r_1 g_{s_1, s_2}^{(1)}(T'_1, T'_2) \sin \left[ (\omega_p^0/c)(z_{p_2} - z_{p_1}) - (\omega_i^0/c)(z_2 + n_i L + 2n_0 d_0) - (\omega_s^0/c)(z_1 - z_3) \right] \right\},$$

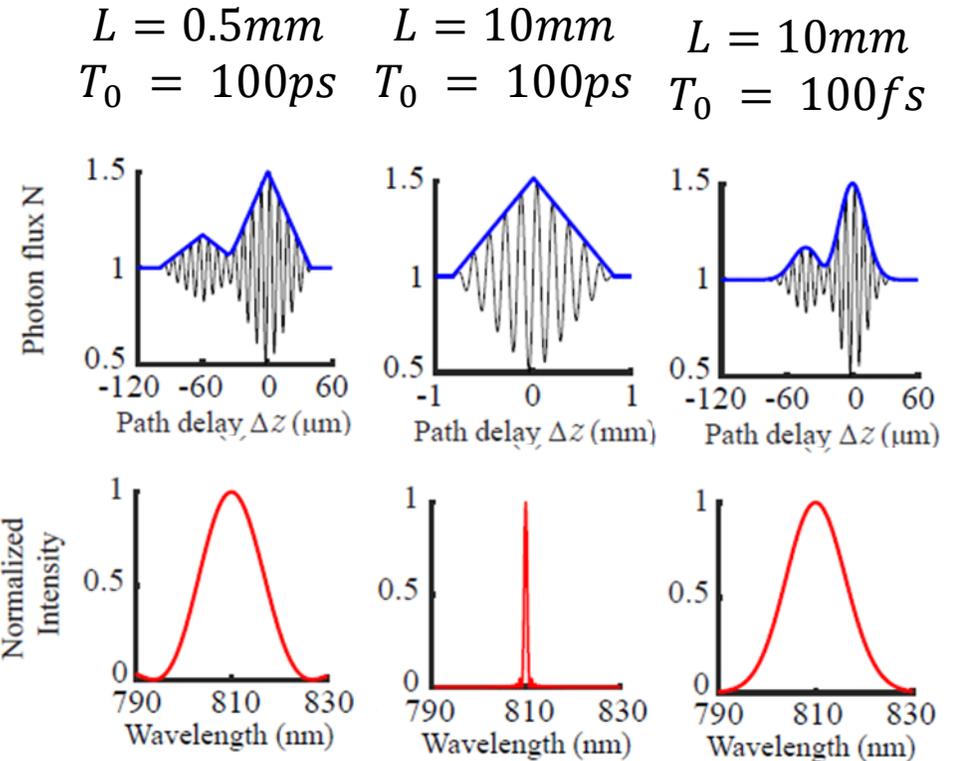


Fig. (Up) Signal detected, In blue the first order correlation function. (down) Normalized spectrum of the signal photon. thickness  $2n_0d$ .



## 5. Conclusions

- We observe coherence for all degrees of entanglement between the signal and idler beams.
- It's possible to achieve high axial resolution and high photon emission rates by combining ultrashort pumping with millimeter length crystals in an induced coherence tomography system.
- The method maintains its salutary features, i.e., probing the sample with photons centered at the most appropriate wavelength while using the optimum wavelength for silicon-based photodetectors.

References in the Preprint arXiv:2005.03741

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